

# Bibliography on Path Analysis in Functional Neuroimaging

Finn Årup Nielsen  
CIMBI at DTU Informatics and NRU Rigshospitalet  
Lyngby and Copenhagen, Denmark

April 23, 2010

\$Revision: 1.58 \$  
\$Date: 2008/10/23 11:28:32 \$

## Abstract

References for *path analysis* (structural equation modeling) and related connectivity analyses (“functional integration”) for functional neuroimaging are collected.

This bibliography is part of a larger collection of bibliographies that was begun in 2001 see <http://www.imm.dtu.dk/~fn/bib/Nielsen2001Bib/>. The bibliography is written in L<sup>A</sup>T<sub>E</sub>X and BIB-TeX and should be available both as HTML, PDF and PostScript:

- <http://www.imm.dtu.dk/~fn/bib/Nielsen2001BibPath/>
- <http://www.imm.dtu.dk/~fn/bib/Nielsen2001BibPath.pdf>
- <http://www.imm.dtu.dk/~fn/bib/Nielsen2001BibPath.ps>

The bibliography is probably far from complete, but new references are added whenever the author finds new material and has the time to add them. You can email the author if corrections are required or you have found some reference that you fell ought to be included: fn@imm.dtu.dk.

Funding is from Lundbeck Foundation, the European Union project MAPAWAMO, International Neuroimaging Consortium (INC) HBM project, THOR Center for Neuroinformatics, the Villum Kann Rasmussen Foundation and the Lundbeck Foundation.

## 1 Terminology

Path analysis in functional neuroimaging is usually used to described the network between brain regions. In functional neuroimaging the term *structural equation modeling* (SEM) is more common. It has also been called *covariance structural equation modelling* (CSEM) (McIntosh and Gonzalez-Lima, 1994b; Taylor et al., 2000). The aspect revealed by path analysis in functional neuroimaging has been termed *effective connectivity* by Karl J. Friston, — in contrast to *functional connectivity* which describes the correlation among brain regions (Friston, 1994, 2004), cf. the related concept in spike train analysis, e.g., (Espinosa and Gerstein, 1988). *Systems-level neural modeling* has also been used to denote path analysis on the large scale brain regions (Horwitz et al., 1999, box on page 92). Analysis of the network dynamics might reveal the *transient response plasticity* (McIntosh, 2000).

## 2 General references

Bollen (1989, 1998b,a) gives general introductions to structural equation modeling and path analysis, and Ferron and Hess (2007) make a concrete example with maximum likelihood estimation for the structural equation model. Sánchez et al. (2005) review structural equation modeling and give an example application in environment epidemiology.

The “Computational approaches to network analysis in functional imaging” special issue of the journal *Human Brain Mapping*, volume 2, numbers 1 and 2, 1994, contains 8 contributions, e.g., (McIntosh and Gonzalez-Lima, 1994b; Gonzalez-Lima and McIntosh, 1994; Grafton et al., 1994; Friston, 1994; Alexander and Moeller, 1994; Horwitz, 1994).

Introductions to path and related analyses in functional neuroimaging are given by Büchel and Friston (1997a,b).

### 3 Analysis types for brain networks

If a broad angle is taken to path analysis a number of different analysis types can be regarded as “path analysis”, e.g., principal component analysis (PCA), ordinary structural equation modeling, see table 1. For independent component analysis (ICA) see the *Bibliography on Independent Component Analysis in Functional Neuroimaging*, <http://www.imm.dtu.dk/~fn/bib/Nielsen2001BibICA/>.

The functional connectivity can be assessed by *cross-correlation analysis between voxels*, also called “seed voxel correlation analysis”. This can be done by selecting a few important voxels and examining their correlation with the rest of the brain. Worsley et al. (1998a,b, 2005a) compute the correlation from all voxels to all voxel and a threshold for on the 6D correlation random field is applied (Cao and Worsley, 1998). Worsley et al. (2005b) compare cross-correlation and SVD.

Table 1: Analysis types for brain networks

Abbrv.	Name	Comments	References
CC	Cross-correlation analysis	Cross-correlation between one region/voxel to another, also: “correlational analysis” or “seed voxel correlation analysis” (SVCA)	Metter et al. (1984b); Horwitz et al. (1984); Cao and Worsley (1998)
	Regression with PCA	Voxel-Voxel regression with principal component analysis	Friston et al. (1993)
CCA	Canonical correlation analysis		Friston et al. (1995a); Bullmore et al. (1996)
CRA	Canonical ridge analysis	Regularization of the canonical correlation analysis model so it can be performed on neuroimaging data	Nielsen et al. (1998)
PLS	Partial least squares		McIntosh and Lobaugh (2004)
PPI	Psychophysiological interaction		Friston et al. (1997)
RAM	Reticular action model		McArdle and McDonald (1984); Steele et al. (2004)
SEM	Structural equation modeling	Also called path analysis	Penny et al. (2004)
RD	Replicator dynamics		Lohmann and Bohn (2002)
SVD	Singular value decomposition	Similar to principal component analysis	Sychra et al. (1994): On fMRI
SSM	Scaled subprofile model		Moeller et al. (1987)
DCM	Dynamic Causal Modeling		Friston et al. (2003); Friston (2003); Penny et al. (2004)

The validity of the inference made by dynamic causal modeling is explored by Lee et al. (2006).

### 3.1 Mathematical description of structural equations model

A general form of structural equations is (Bollen, 1989, eqs. 2.4, 2.8 and 2.9):

$$\mathbf{N} = \mathbf{NB} + \mathbf{\Xi}\boldsymbol{\Gamma} + \mathbf{Z} \quad (1)$$

$$\mathbf{X} = \mathbf{\Xi}\boldsymbol{\Lambda}_x + \mathbf{\Delta} \quad (2)$$

$$\mathbf{Y} = \mathbf{N}\boldsymbol{\Lambda}_y + \mathbf{E} \quad (3)$$

The first equation is for the latent variables, while the second and third equations (“the measurement model”) relate the latent variables to the observed variables,  $\mathbf{X}$  and  $\mathbf{Y}$ . The diagonal of  $\mathbf{B}$  should be zero.

If there is no measurement noise,  $\mathbf{\Delta} = \mathbf{0}$  and  $\mathbf{E} = \mathbf{0}$ , and there is a one-to-one relationship between the latent and observed variables,  $\boldsymbol{\Lambda}_x = \mathbf{I}$  and  $\boldsymbol{\Lambda}_y = \mathbf{I}$ , then the structural equations can be written as

$$\mathbf{Y} = \mathbf{YB} + \mathbf{X}\boldsymbol{\Gamma} + \mathbf{Z} \quad (4)$$

In econometrics one finds the so-called “structural form” in “simultaneous equation systems” (Mardia et al., 1979, section 7.3, equation 7.3.1)

$$\mathbf{YB} + \mathbf{X}\boldsymbol{\Gamma} = \mathbf{U} \quad (5)$$

This is equivalent to equation 4 with suitable redefinitions, e.g.,  $\mathbf{B} \rightarrow \mathbf{I} - \mathbf{B}$ ,  $\boldsymbol{\Gamma} \rightarrow -\boldsymbol{\Gamma}$  and  $\mathbf{Z} \rightarrow \mathbf{U}$ .

$\mathbf{\Xi}$  and  $\mathbf{X}$  are called the *exogenous* or independent variables while  $\mathbf{N}$  and  $\mathbf{Y}$  are called the *endogenous* variables. If there are no exogenous variables,  $\mathbf{X} = \mathbf{0}$ , then equation 4 simplifies to

$$\mathbf{Y} = \mathbf{YB} + \mathbf{Z} \quad (6)$$

When regarding this equation as a network the columns of the  $\mathbf{Y}$  are the nodes of the network, while the  $\mathbf{B}$  matrix describes the links between the nodes.

#### 3.1.1 Functional neuroimaging

Functional neuroimaging tends to use the relatively simple equation 6, though, e.g., with this renaming

$$\mathbf{X} = \mathbf{XK} + \mathbf{U} \quad (7)$$

Most often  $\mathbf{X}(N \times P)$  will contain data from brain scannings, e.g., as a  $\mathbf{X}(\text{scans} \times \text{brain regions})$  matrix, while  $\mathbf{K}(\text{brain regions} \times \text{brain regions})$  is the “network” one wants to estimate and this is typically regarded as sparse, i.e., many elements are zero.

An example taken from (Bullmore et al., 2000, page 295) with a transposed notation for a single scan

$$\mathbf{x}_{(n)}^T = \mathbf{K}^T \mathbf{x}_{(n)}^T + \mathbf{u}_{(n)}^T \quad (8)$$

$$\begin{bmatrix} \text{VEC} \\ \text{PFC} \\ \text{SMA} \\ \text{IFG} \\ \text{IPL} \end{bmatrix} = \begin{bmatrix} 0 & 0 & 0 & 0 & \theta_1 \\ \theta_2 & 0 & 0 & 0 & 0 \\ 0 & \theta_3 & 0 & 0 & 0 \\ 0 & 0 & \theta_4 & 0 & 0 \\ \theta_6 & 0 & 0 & \theta_5 & 0 \end{bmatrix} \times \begin{bmatrix} \text{VEC} \\ \text{PFC} \\ \text{SMA} \\ \text{IFG} \\ \text{IPL} \end{bmatrix} + \begin{bmatrix} \psi_1 \\ \psi_2 \\ \psi_3 \\ \psi_4 \\ \psi_5 \end{bmatrix} \quad (9)$$

In this kind of application of structural equation modeling the brain regions are the nodes of the network. Multisubject extension to this scheme make nodes also over subject so the matrix  $\mathbf{X}$  gets the size (scans  $\times$  (brain regions  $\times$  subjects)) (Mechelli et al., 2002).

#### 3.1.2 Number of networks

The number of different networks (in terms of zero structure) for even small sized structure matrices is very large. For a two-by-two structure matrix,  $\mathbf{K}(2 \times 2)$ , there are 3 non-zero networks and 4 if we allow for the zero network: There are two elements of the structure matrix that can either be zero or non-zero

independent of each other. This gives all combinations:  $2^2 = 4$ . Generally, for a  $N$ -by- $N$  structure matrix,  $\mathbf{K}(N \times N)$ , the form for the number of networks  $L(N)$  is:

$$L(N) = 2^{N \times N - N} = 2^{N(N-1)} \quad (10)$$

Some examples:  $L(3) = 64$ ,  $L(4) = 4\,096$ ,  $L(5) = 1\,048\,576$ ,  $L(6) = 1\,073\,741\,824$ .

If one considers a growing network where one non-zero element in the structure matrix is added at a time, and when a non-zero element is added it is maintained in the network, then the number of possible networks shrinks dramatically. The number of possible non-zero elements to start with is  $M = N(N-1)$ . When the first element is added and the network is incremented with a new non-zero element then there are  $M-1$  elements left to choose from. In the next step only  $M-2$  and so on until the all off-diagonal element of the structure matrix is non-zero. The form for the total number of networks that is traversed is

$$L_{\text{grow}}(N) = \sum_{m=0}^M (M-m) = M(M+1) - \frac{M(M+1)}{2} = \frac{M(M+1)}{2} \quad (11)$$

$$= \frac{N(N-1)(N(N-1)+1)}{2} = \frac{N^4 - 2N^3 + 2N^2 - N}{2} \quad (12)$$

Some examples:  $L_{\text{grow}}(2) = 3$ ,  $L_{\text{grow}}(3) = 21$ ,  $L_{\text{grow}}(4) = 78$ ,  $L_{\text{grow}}(5) = 210$ ,  $L_{\text{grow}}(6) = 465$  and  $L_{\text{grow}}(7) = 903$ .

### 3.2 Other remarks

*Panel analysis* is a dynamic (longitudinal) form of path analysis, see, e.g., Easdon and McIntosh (2000) for an application in functional neuroimaging. Büchel et al. (1999) investigated the change in path coefficients over time in associative learning.

Structural equation modeling on BOLD fMRI may be confounded by 1/f-noise and/or cardiac and respiratory noise that can cause nuisance connectivity, see, e.g., a comment by Lund (2001).

### 3.3 Tools

Some of the few tools that enable path and related analyses are listed in table 2. Haughton et al. (2006) describes three software packages for directed acyclic graphs: MIM, Tetrad and WinMine.

Table 2: Analysis types for brain networks.

Name	Description	References
gR	Graphical modeling in R	
LiNGAM	“Discovery of non-gaussian linear causal models” matlab programs	Shimizu et al. (2006), <a href="http://www.cs.helsinki.fi/group/neuroinf/lingam/">http://www.cs.helsinki.fi/group/neuroinf/lingam/</a>
MIM		Edwards (2000, 1995), <a href="http://www.hypergraph.dk">http://www.hypergraph.dk</a> ,
Mplus	Commercial windows program for structural equations modeling	Muthén and Muthén (2006), <a href="http://www.statmodel.com/">http://www.statmodel.com/</a>
Mx	Binary programs for Linux, Mac, Unix and Windows	Neale et al. (2003), <a href="http://www.vcu.edu/mx/">http://www.vcu.edu/mx/</a>
SEM (Steele)	Structural equation modeling implemented in Matlab by J. Douglas Steele	<a href="http://www.abdn.ac.uk/~men204/SEM.htm">http://www.abdn.ac.uk/~men204/SEM.htm</a>
SPM2 DCM	Dynamic Causal Modeling as implemented in SPM2	Friston et al. (2003); Friston (2003)
LISREL	Commercial general structural equation modeling program	<a href="http://www.ssicentral.com/other/entry.htm">http://www.ssicentral.com/other/entry.htm</a>

Name	Description	References
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## 4 Applications

Some early examples: Høedt-Rasmussen and Skinhøj (1964) compared hemispheric cerebral blood flow based on measurements with Krypton-85. Paulson (1970); Paulson et al. (1970) compute the “interchannel coefficient of variation” (or “interregional coefficient of variation”) between 16 channels measuring cerebral blood flow with Xenon-133.

Most studies analyze functional brain scans. However, there has also been a study that considered the covariance between gray matter density in different brain regions via voxel-based morphometry (Mechelli et al., 2005). .

Table 3: Path analyses in functional neuroimaging. VEC: ventral extrastriate cortex, PFC: prefrontal cortex, SMA: supplementary motor area, IFG: Interior frontal gyrus, IPL: Inferior parietal lobe.

Type	Scan	Variables-/Regions	Behavioral domain	Remarks	Reference
—	—	—	—	Review	McIntosh (1999) Horwitz et al. (1999)
—	—	—	—	Review	Taylor et al. (2000)
—	—	—	Overview	Brief description in section 3.1	Horwitz et al. (2000a)
CC	PET	2 × 23 + 3	Resting	Partial correlation, kappa statistics	Horwitz et al. (1984)
CC	PET	2 × ?	Normals		Metter et al. (1984b)
CC	PET	2 × ?	Resting	Normals, Alzheimer, Huntington, Parkinson	Metter et al. (1984a)
SEM	PET	2 × 7: BA 17/18, 19d, 19v, 7, 37, 21, 46	Object and spatial vision		McIntosh and Gonzalez-Lima (1994b); McIntosh et al. (1994)
?	?	?	?	?	Horwitz (1994)
SEM	PET	5: SMA/cing, motor, putamen, GP, thalamus	Movement	Controls and Parkinson’s disease patients	Grafton et al. (1994)
CC	fMRI		Vision		Kleinschmidt et al. (1994)
CC	fMRI	?	Resting state		Biswal et al. (1995)
SEM	PET	?	Face matching with Alzheimer patients		Horwitz et al. (1995)
CC/SEM	PET	11 regions	reading, visual word recognition		Nyberg et al. (1996)

Type	Scan	Variables-/Regions	Behavioral domain	Remarks	Reference
SEM	fMRI	?	Visual motion	Modulation modeled with interaction term	Büchel and Friston (1997c)
?	PET	?	Semantic processing in schizophrenia		Jennings et al. (1998)
CC	PET		Reading and dyslexia		Horwitz et al. (1998)
CC	PET	All voxels	Vigilance task	Correlation field threshold via random field theory	Worsley et al. (1998a,b)
SEM	fMRI	$2 \times 7$	Motor task	Low-frequency BOLD fMRI	Lowe (1999)
?	PET	?	Face encoding and recognition		Rajah et al. (1999)
?	PET	?	Episodic encoding and retrieval of words		Krause et al. (1999)
?	fMRI	?	Associative learning		Büchel et al. (1999)
CC	fMRI	A few voxels in hippocampus and thalamus	Resting state		Stein et al. (2000)
?	PET		Language processing		Petersson et al. (2000)
CC	PET	Wernicke, Broca, others	Language production		Horwitz et al. (2000b)
CC	fMRI	Voxels in Rolandic cortex, ventrolateral thalamus, anterior putamen correlated with the rest of the brain	Motor		Mopritz et al. (2000)
Panel/PLS	PET	Left cerebellum, left superior frontal cortex	Eyeblink conditioning		Easdon and McIntosh (2000)
PLS	PET		Short-term memory wrt. age		Della-Maggiore et al. (2000)
SEM	fMRI	5: VEC, PFC, SMA, IFG, IPL	Semantic decision, subvocal rehearsal	Model order determination by P-values, AIC and Bollen's "parsimonious fit index"	Bullmore et al. (2000)
SEM	fMRI	7	Memory retrieval		Maguire et al. (2000)
SEM	PET	?	?		Nezafat et al. (2001)

Type	Scan	Variables-/Regions	Behavioral domain	Remarks	Reference
CC	fMRI	From/to anterior cerebellum	Simple motor task	Schizophrenia and control subjects	Stephan et al. (2001)
?	fMRI	9: EC, BA37, IPS, SMA, FEF, VPC, IFG, PSTS, AG	Implicit language processing		?
SEM	PET	12	Working memory	Split-half validation, AIC and RMSEA	Glabus et al. (2003)
PLS	?	39		FDG, rats,	Nair and Gonzalez-Lima (2003)
SEM	fMRI	10	Visual attention	In normals and Williams syndrome	Meyer-Lindenberg et al. (2004)
RAM	fMRI	5	Predictive error signal	Depressive illness	Steele et al. (2004)
CC	fMRI	Voxels	Finger opposition	Power law, clustering coefficient and path length computed (small world variables)	Eguíluz et al. (2005)
SEM	fMRI	10	Flanker task (attentional control)		Erickson et al. (2005)
SEM	fMRI	4	Emotional face processing	In normals and Williams syndrome	Meyer-Lindenberg et al. (2005)
SEM	fMRI	8 regions around amygdala	Negative emotional faces	Minimization with adaptive simulated annealing and with split half verification	Stein et al. (2006)
CC	fMRI	90 regions	Resting state with pharmacological stimulation	Wavelet correlation analysis in the frequency interval 0.06–0.11 and with metrics of network efficiency (small world)	Achard and Bullmore (2007)
SEM	MRI		None	Size of brain regions	Colibazzi et al. (2008)

## 4.1 Resting state path analysis

Functional connectivity has been assessed with resting state BOLD fMRI (Biswal et al., 1995), e.g., Stein et al. (2000) pick a few seed voxels in the thalamus and the hippocampus and compute the correlation coefficient between these (each at a time) and the rest of the brain, thresholding at 0.5. The correlation is high for low frequencies (< 0.1 Hz), and hypercapnia results in a substantial decrease in the correlation (Biswal et al., 1997). Lowe et al. (1998) report low-frequency resting state fluctuation with low sampling rate multislice. Xiong et al. (1999) pick the seed in the primary motor cortex.

## 4.2 Unclassified

Kim et al. (2007): MAR, SEM, GLM  
Clark et al. (1984)  
Koch et al. (2002): Comparison of functional and anatomical connectivity.  
McIntosh and Gonzalez-Lima (1991): SEM on auditory system.  
McIntosh and Gonzalez-Lima (1992): SEM on the visual system of the rat.  
McIntosh and Gonzalez-Lima (1994a)  
Anatomically based structural equation modeling (SEM) Rajah et al. (1999)  
Friston et al. (1995b) “regression”.  
Cordes et al. (2001)  
(Büchel and Friston (1998): “variable parameter regression” and Kalman filtering)  
Cordes 2000, AJNR, 21:1636

### 4.2.1 ”Structural equation” and PET

From PubMed: Nezafat et al. (2001), Della-Maggiore et al. (2000), Petersson et al. (2000), Taylor et al. (2000), McIntosh (1999), Rajah et al. (1999), Horwitz et al. (1999), McIntosh (1998), Jennings et al. (1998), Cabeza et al. (1997), McIntosh et al. (1994).

## 5 Other connectivity analyses

Brain connectivity may also be obtained from tractography of diffusion spectrum imaging (Hagmann et al., 2008).

## A Examples of networks

### A.1 Object and spatial vision

The following functional networks are originally from McIntosh et al. (1994). The network descriptions are in the *dot* file format Koutsos and North (1996) and figures 1 and 2 display the output from the program. Negative path coefficients are indicated by dotted lines.

```
digraph ObjectVision {
    rankdir=LR
    "17/18" -> "19v"
    "17/18" -> "19d" [style=dotted]
    "19v" -> "37"
    "19v" -> "19d"
    "19d" -> "7" [style=dotted]
    "19d" -> "46" [style=dotted]
    "37" -> "21"
    "37" -> "7" [style=dotted]
    "7" -> "21"
    "7" -> "46" [style=dotted]
    "21" -> "46"
    "46" -> "19v" [style=dotted]
}
```

```
digraph SpatialVision {
    rankdir=LR
    "17/18" -> "19v"
    "17/18" -> "19d"
    "19v" -> "37"
    "19v" -> "19d"
    "19d" -> "7"
```

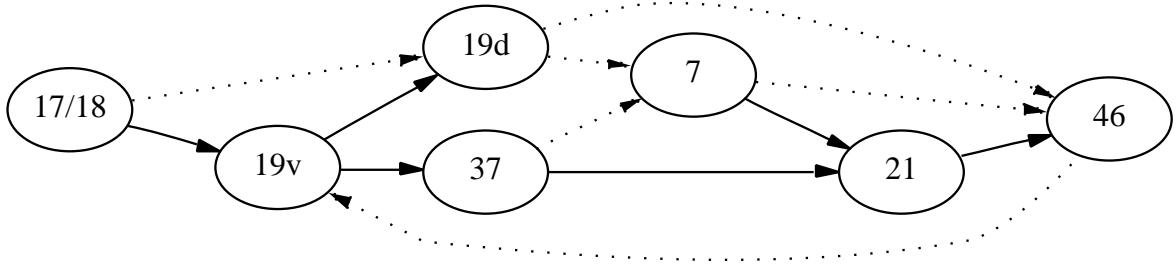


Figure 1: Object vision functional network for the right hemisphere. Adapted from (Horwitz, 1994, figure 3) which is adapted from McIntosh et al. (1994).

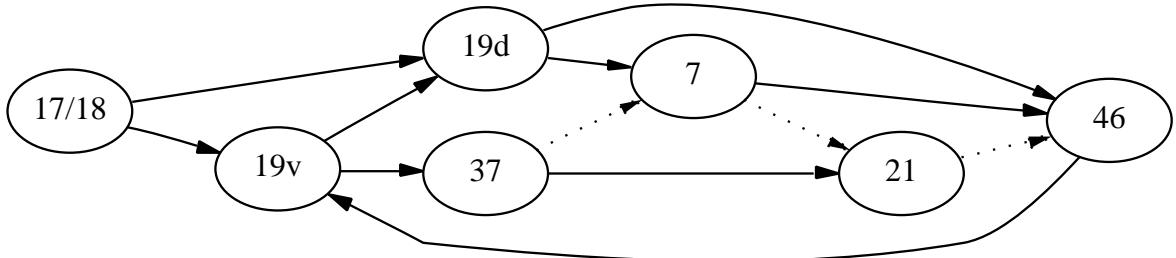


Figure 2: Spatial vision functional network for the right hemisphere. Adapted from (Horwitz, 1994, figure 3) which is adapted from McIntosh et al. (1994).

```

"19d" -> "46"
"37" -> "21"
"37" -> "7" [style=dotted]
"7" -> "21" [style=dotted]
"7" -> "46"
"21" -> "46" [style=dotted]
"46" -> "19v"
}

```

McIntosh and Gonzalez-Lima (1994b) consider interhemispheric functional models for the same task.

## A.2 Motor system

Motor system connectivity is examined by Grafton et al. (1994) who used a cortical-subcortical network proposed by Alexander et al. (1990); DeLong (1990). Some of the results from a LISREL estimation are displayed in figure 3 and the corresponding *dot* file is shown below.

```

digraph GraftonS1994Network {
    subgraph clusterNormalMovement {
        label="Normal subjects, Movement task";
        ranksep=0.75;
        { rank = same;
            NM1 [label="SMA & Cingulate\n Motor Areas" ];
            NM2 [label="Motor cortex"];
    }
}

```

```

        }
        NM3 [label="Putamen"]
        { rank = same;
            NM4 [label="Globus pallidus"];
            NM5 [label="Ventrolateral\n Thalamus"];
        }
        NM1 -> NM2
        NM1 -> NM3 [style=dotted]
        NM1 -> NM5
        NM2 -> NM3 [style=dotted]
        NM2 -> NM5 [style=dotted]
        NM3 -> NM4
        NM4 -> NM5
        NM5 -> NM1
        NM5 -> NM2 [style=dotted]
    }
    subgraph clusterParkinsonBefore {
        label="Parkinson patients, before pallidotomy";
        ranksep=0.75;
        { rank = same;
            PB1 [label="SMA & Cingulate\n Motor Areas" ];
            PB2 [label="Motor cortex"];
        }
        PB3 [label="Putamen"]
        { rank = same;
            PB4 [label="Globus pallidus"];
            PB5 [label="Ventrolateral\n Thalamus"];
        }
        PB1 -> PB2
        PB1 -> PB3 [style=dotted]
        PB1 -> PB5
        PB2 -> PB3
        PB2 -> PB5
        PB3 -> PB4
        PB4 -> PB5
        PB5 -> PB1
        PB5 -> PB2
    }
}

```

### A.3 Cognition

A visual implicit language processing network:

```

digraph McKiernanK2001Development {
    rankdir=LR
    IFG -> VPC
    SMA -> VPC
    FEF -> SMA
    FEF -> VPC
    FEF -> IPC
    PSTS -> IFG
    PSTS -> FEF
    PSTS -> AG
    AG -> IFG [style=dotted]
    IPS -> IFG

```

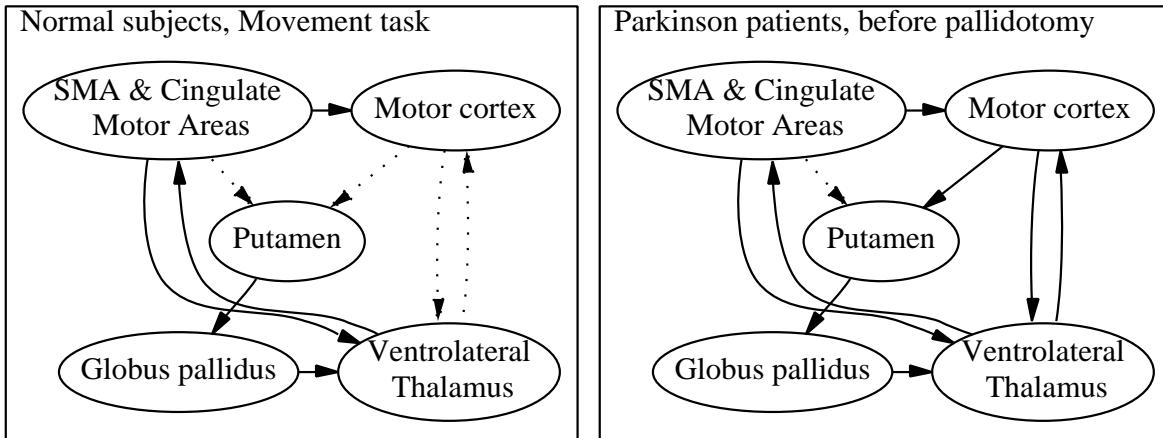


Figure 3: Movement network from Grafton et al. (1994).

```

IPS -> VPC
IPS -> AG
BA37 -> PSTS
BA37 -> VPC [style=dotted]
BA37 -> IPS
EC -> BA37
}

```

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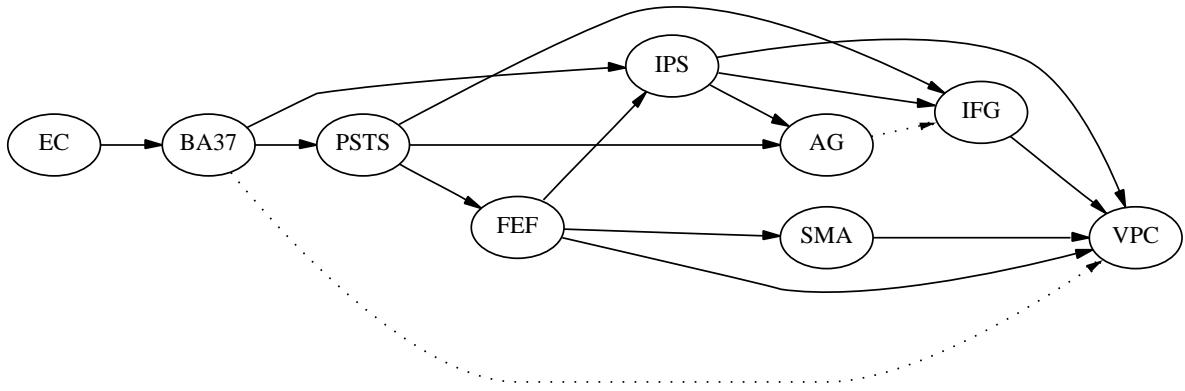


Figure 4: Visual implicit language processing McKiernan et al. (2001).

Büchel, C., Coull, J. T., and Friston, K. J. (1999). The predictive value of changes in effective connectivity for human learning. *Science*, 283(5407):1538–1541. PMID: 10066177. ISSN 0036-8075.

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